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Easley

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(54) **SYSTEMS AND METHODS FOR VITRECTOMY**

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A61F 9/00 (2006.01)

A61F 9/007 (2006.01)

(52) **U.S. Cl.**

CPC **A61F 9/00763** (2013.01); **A61B 50/31** (2016.02); **A61F 9/00736** (2013.01)

(58) **Field of Classification Search**

None

See application file for complete search history.

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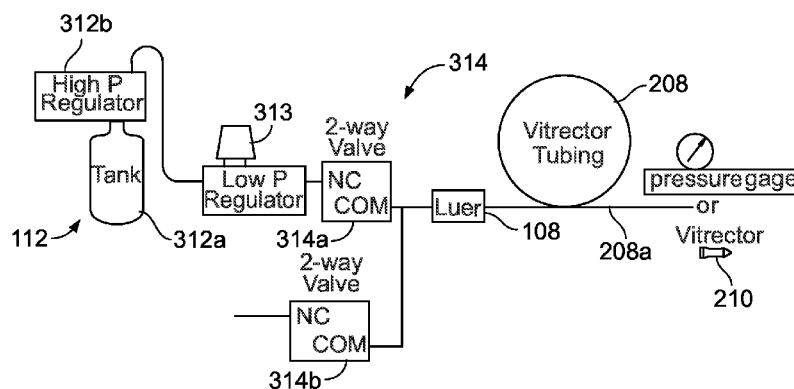
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(57)

ABSTRACT

A system for conducting a vitrectomy includes: a gas source; a vitrector including a cutting mechanism that opens and closes according to a pressure at the vitrector; and a pulse-generating system receiving gas from the gas source and generating pulses at the vitrector. The pulses cause the pressure at the vitrector to vary according to a cycle, and the varying pressure at the vitrector causes the cutting mechanism of the vitrector to open and close. At a first time in the cycle, the pulse-generating system, raises the pressure at the vitrector to a maximum pressure. At a second time in the cycle, the pulse-generating system reduces the pressure at the vitrector to a minimum pressure that is greater than ambient, the pressure at the vitrector being maintained at least at the minimum pressure. The difference between the maximum pressure and minimum pressure is minimized to reduce gas consumption.

17 Claims, 11 Drawing Sheets



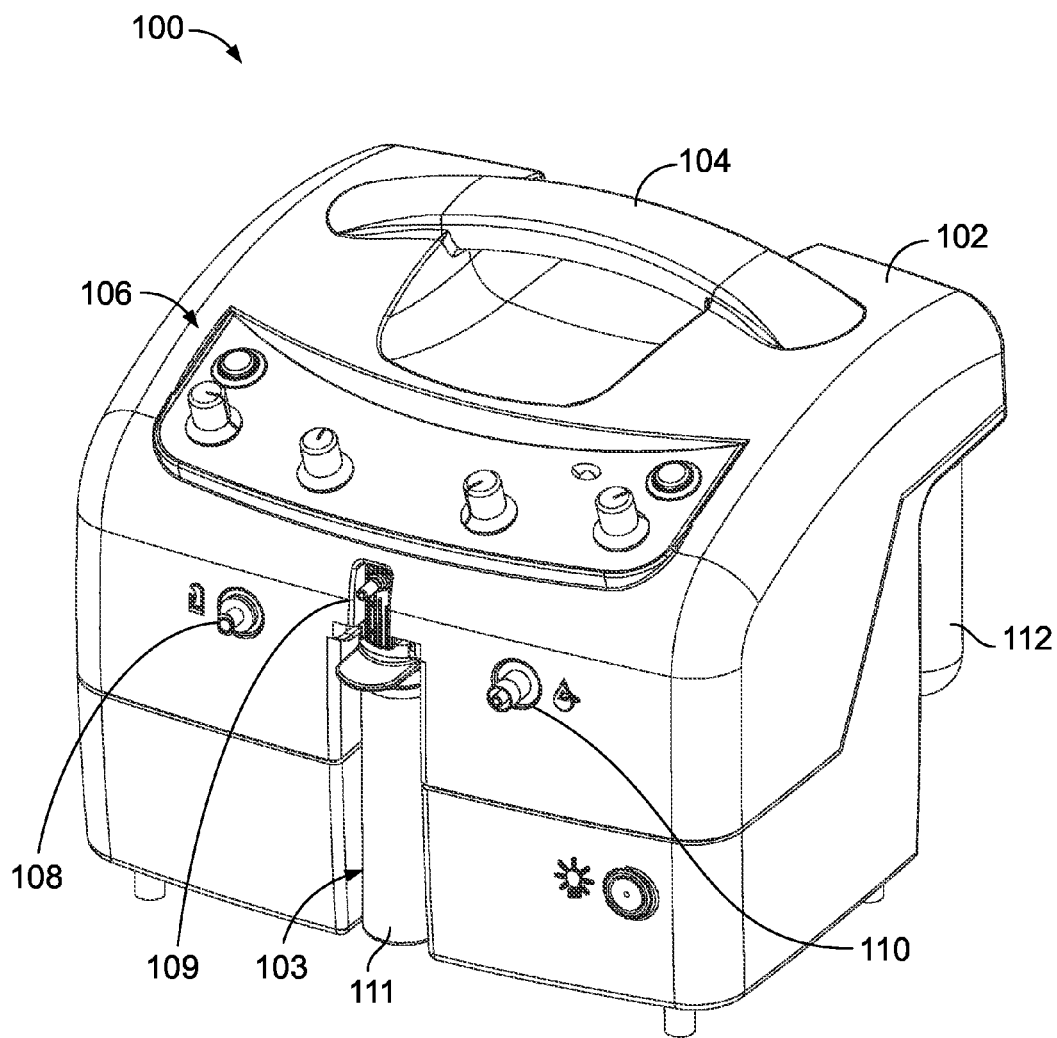
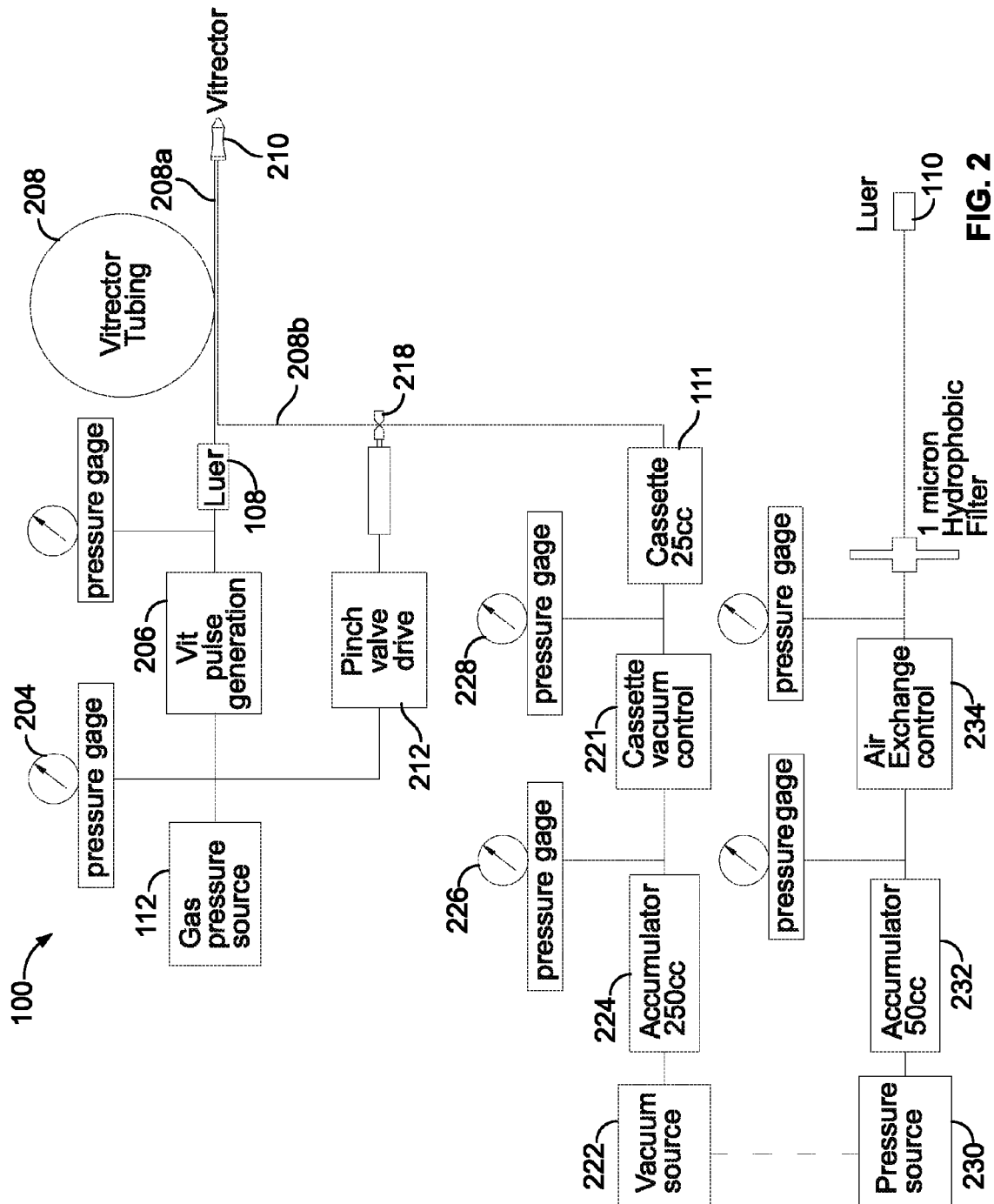


FIG. 1



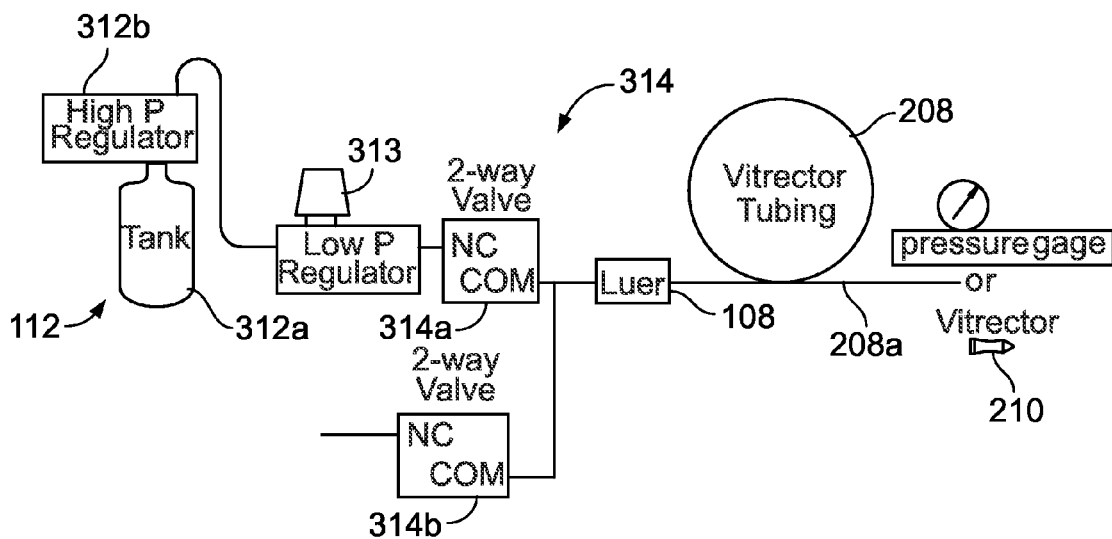


FIG. 3A

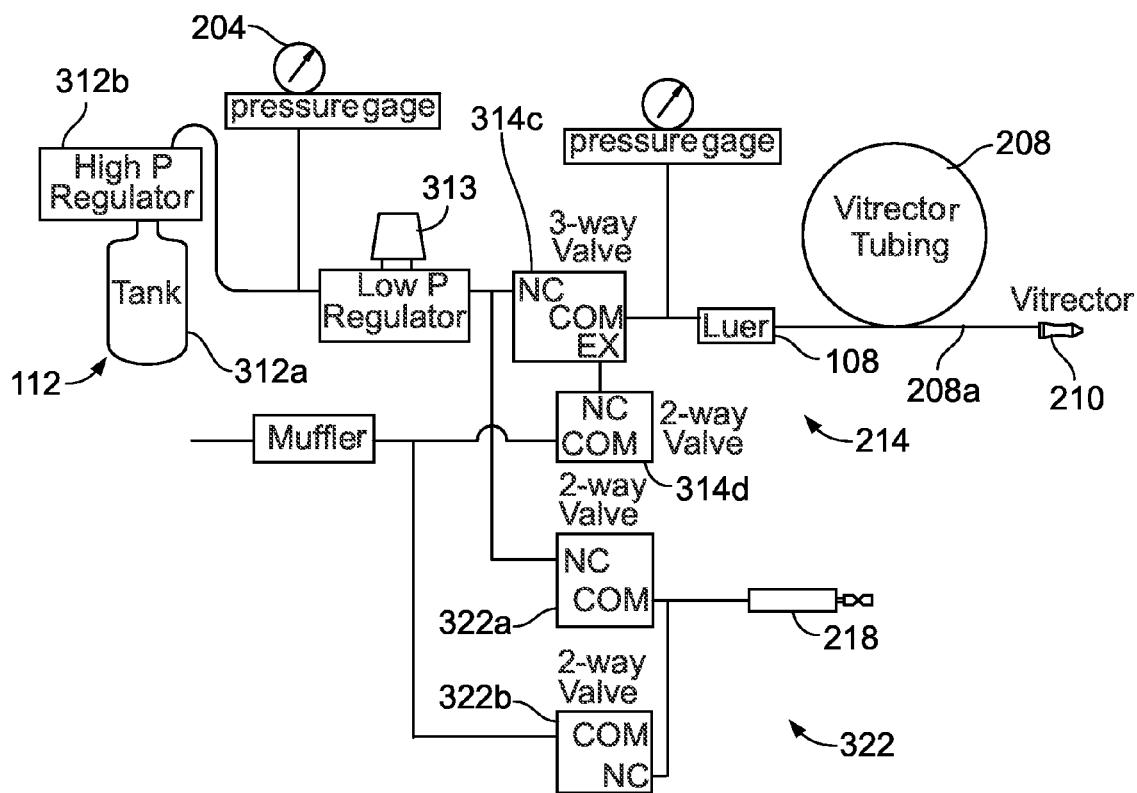


FIG. 3B

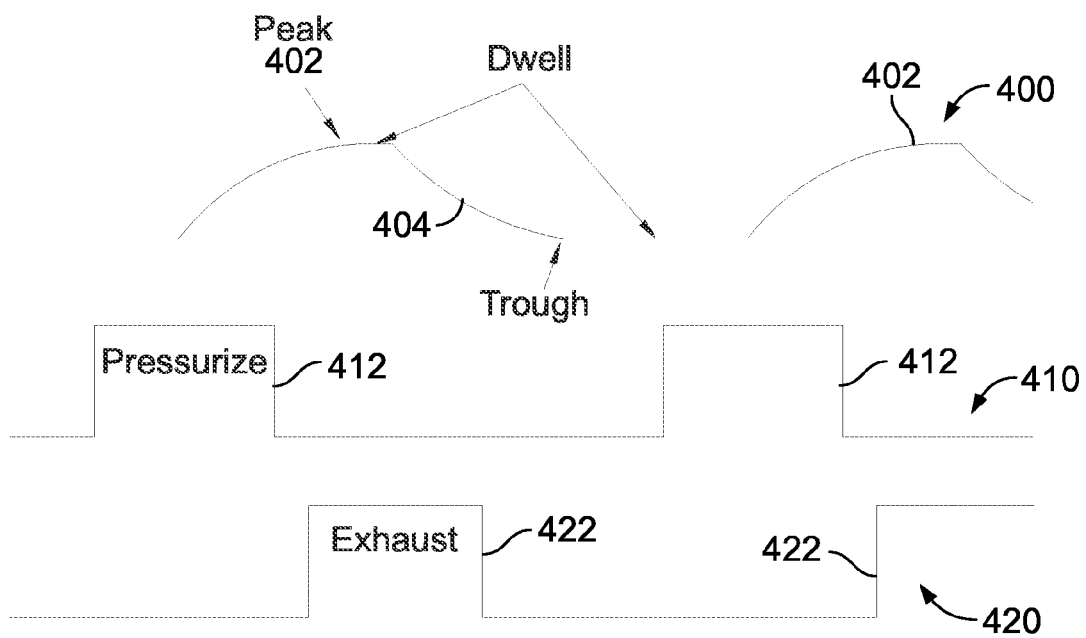


FIG. 4

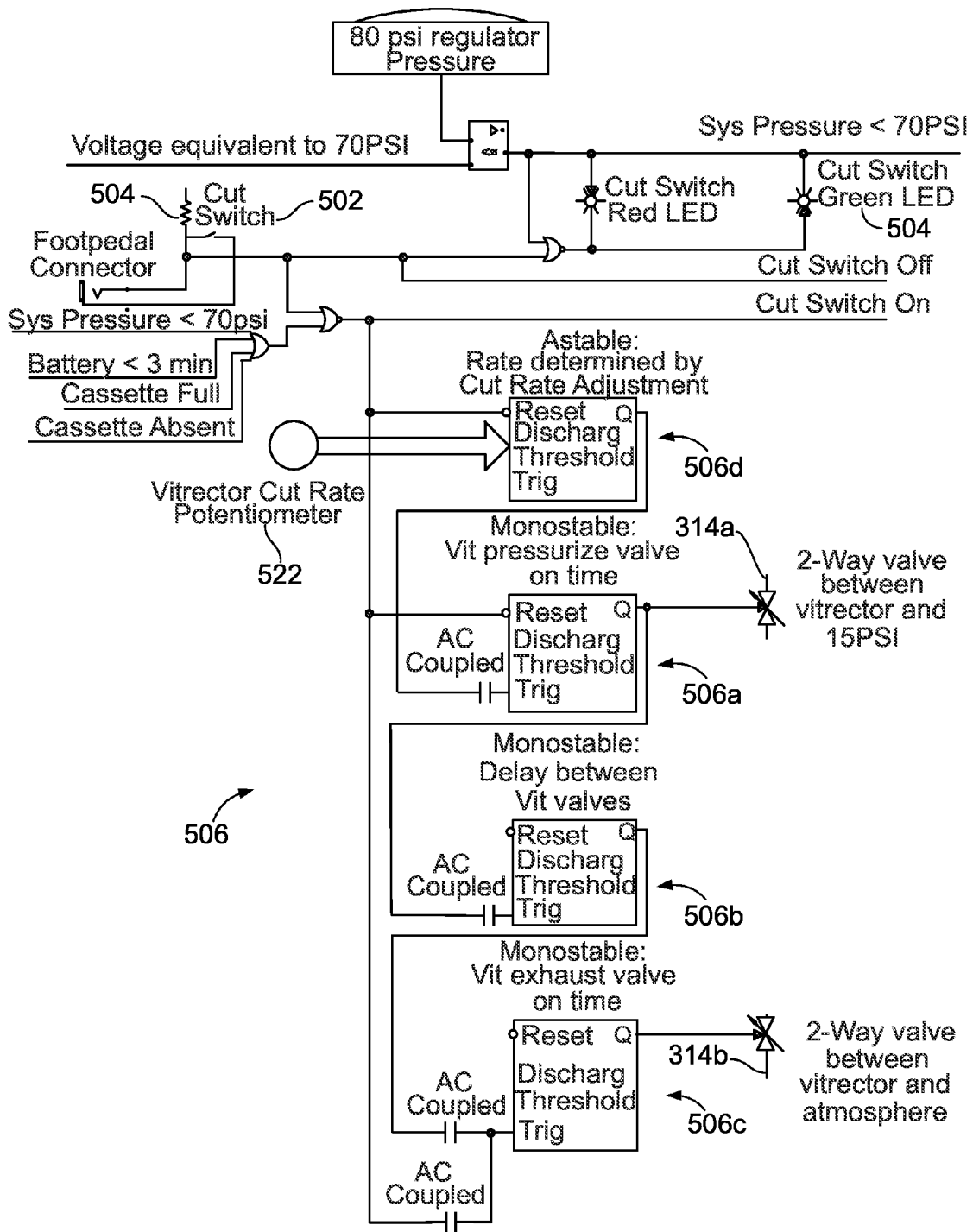


FIG. 5

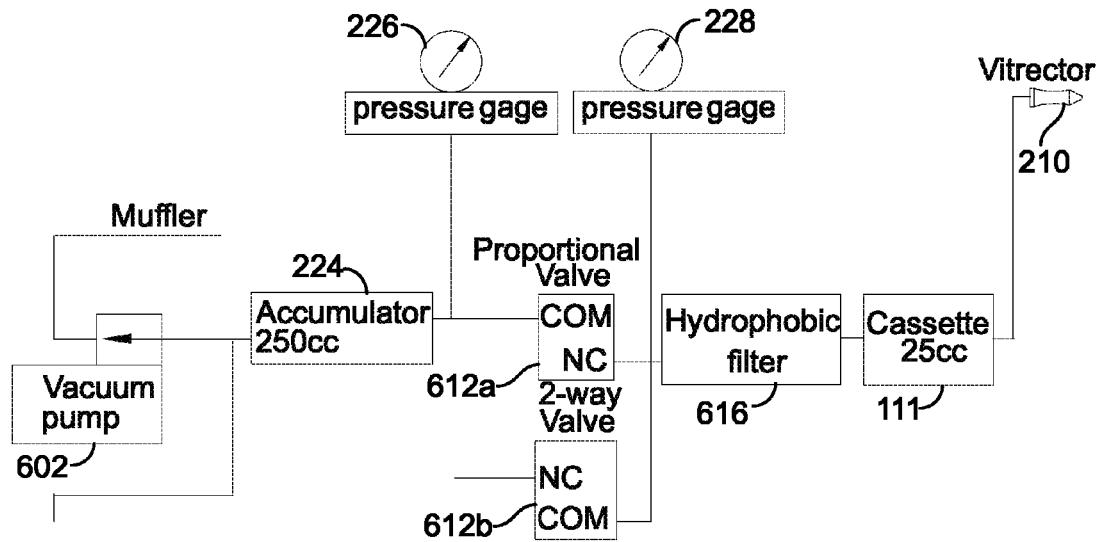


FIG. 6

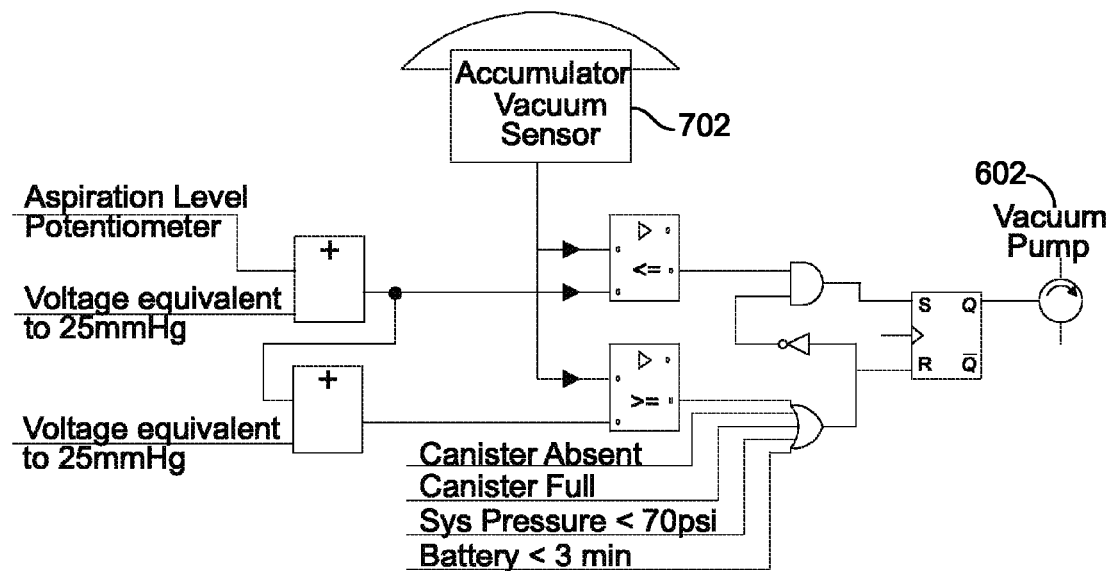


FIG. 7

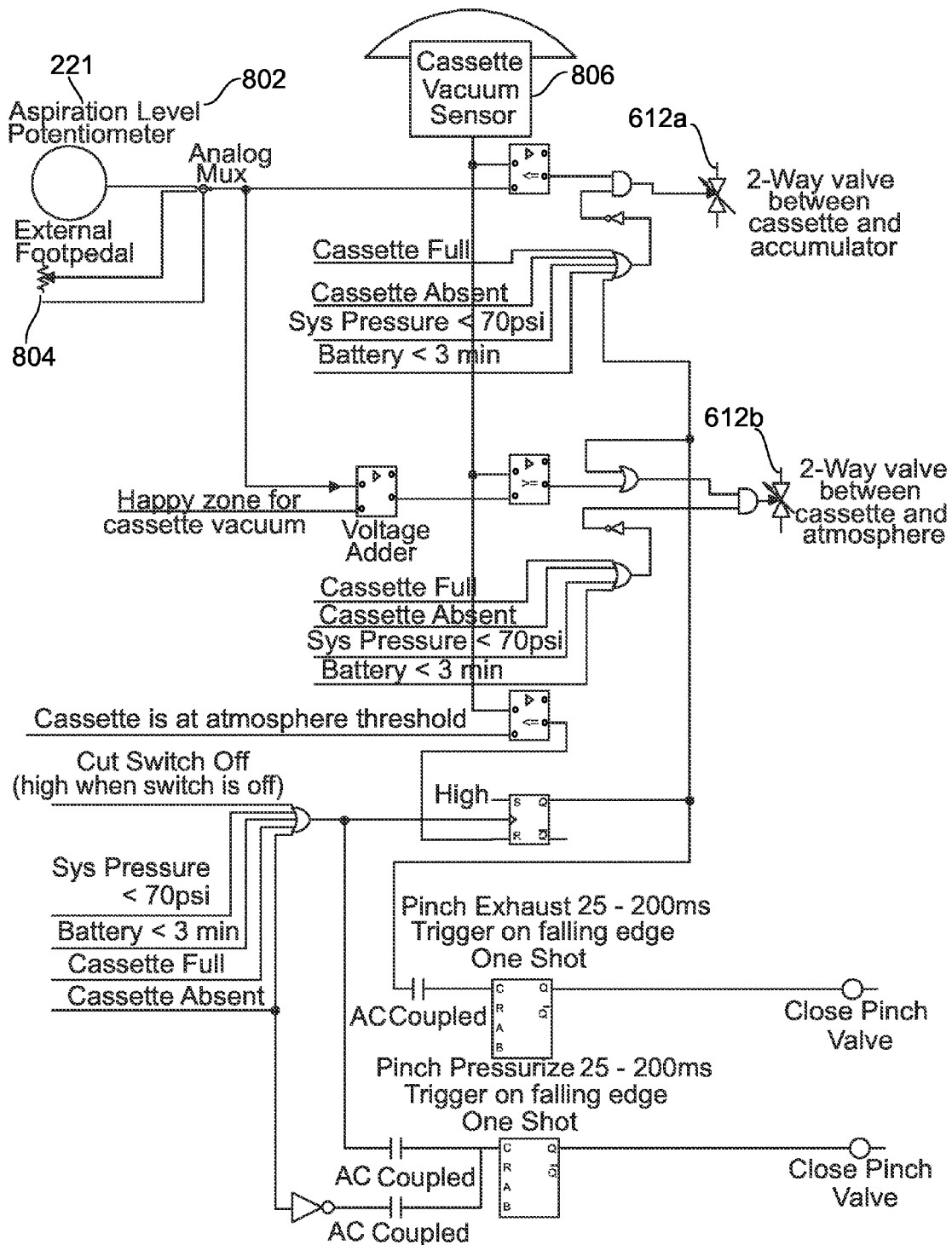


FIG. 8

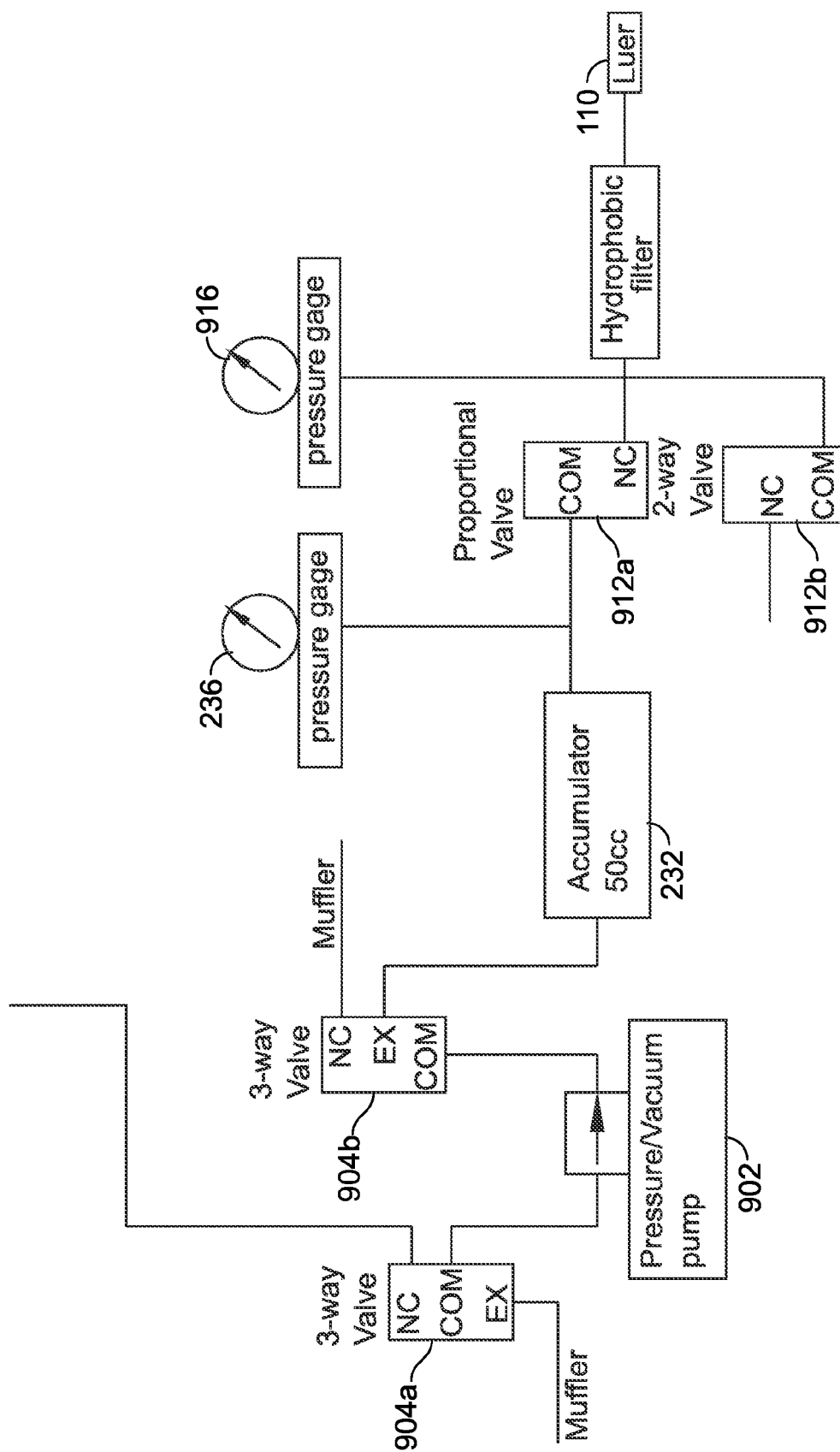


FIG. 9

FIG. 11

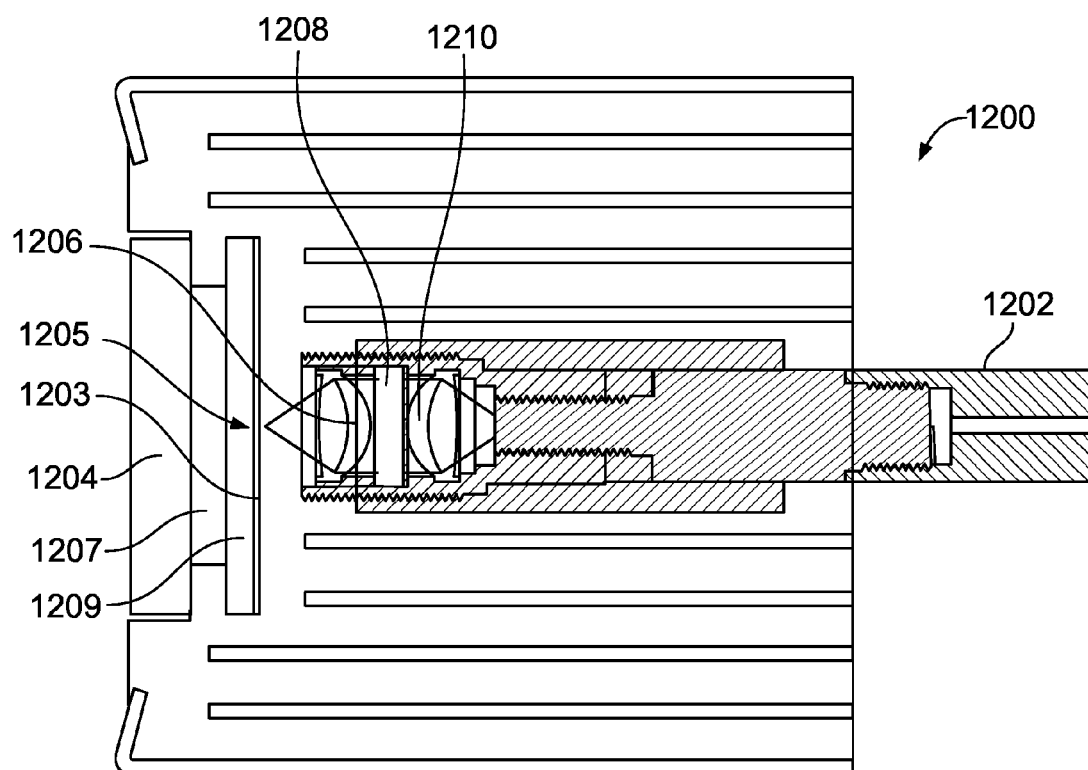
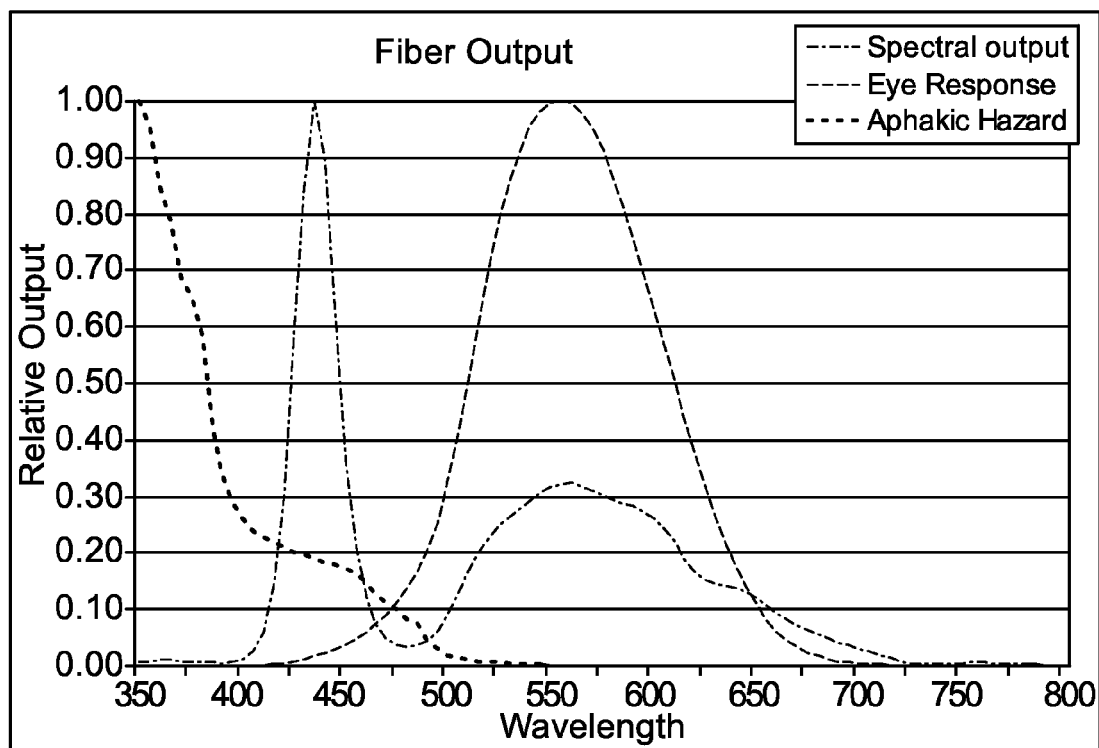
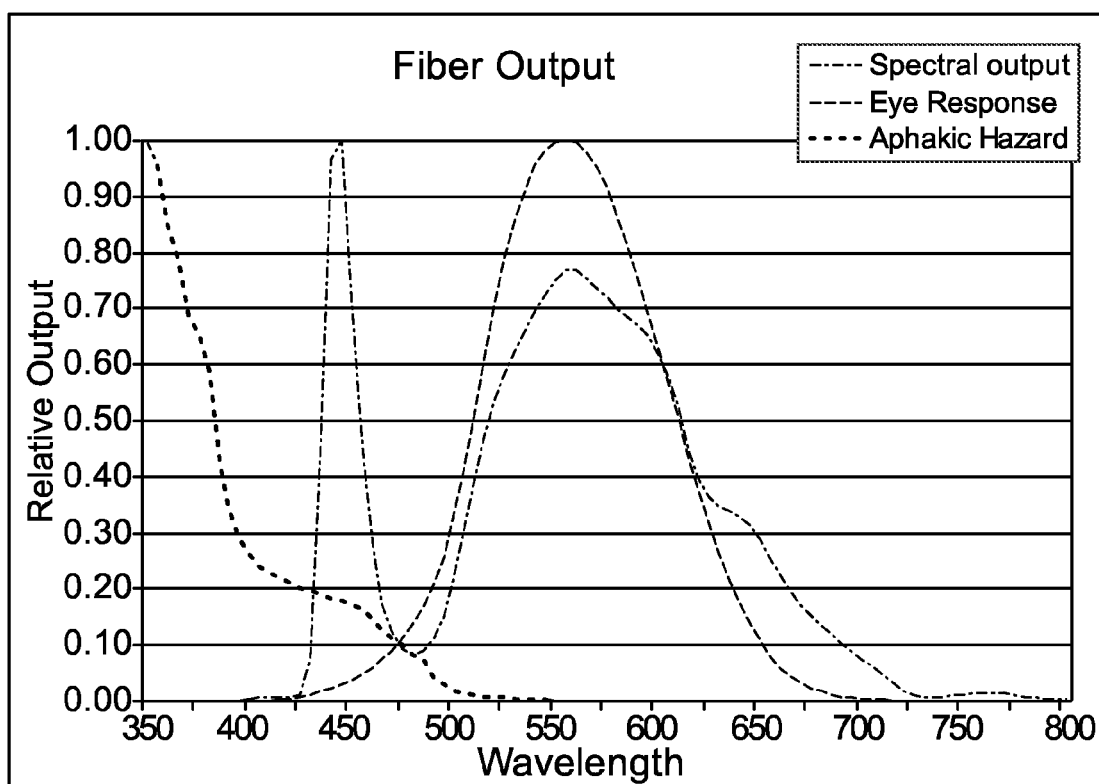


FIG. 12A

**FIG. 12B****FIG. 12C**

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SYSTEMS AND METHODS FOR VITRECTOMY

CROSS REFERENCE TO RELATED APPLICATIONS

This application is a continuation of U.S. application Ser. No. 13/153,912, filed on Jun. 6, 2011, and issued as U.S. Pat. No. 8,496,681 on Jul. 30, 2013, the contents of which are incorporated entirely herein by reference.

BACKGROUND OF THE INVENTION

1. Field of the Invention

The invention pertains to vitrectomy, and more particularly, to portable systems and methods that allow vitrectomy to be conducted in a wide variety of clinical environments.

2. Description of Related Art

Vitrectomy is the surgical removal of vitreous gel from the middle of the eye. Vitreous gel (also called vitreous humor) is a thick, colorless, gel-like fluid that fills the large space in the middle of the eye, behind the lens. Vitreous gel helps the eyeball maintain its shape.

Removal of the vitreous gel, in some cases, provides better access to the back of the eye for particular treatments. For example, vitrectomy provides access for repairing or preventing traction retinal detachment, repairing very large tears in the retina, or treating severe proliferative retinopathy. Vitrectomy may also be employed to reduce vision loss caused by severe or prolonged bleeding in the vitreous gel (vitreous hemorrhage).

Vitrectomy involves three functions: cutting, suction, and infusion. During vitrectomy, small incisions are made in the wall of the eye, through which various instruments are passed. In particular, the doctor inserts a working instrument, e.g., a vitrector, into the eye, cuts the vitreous gel, and suctions the vitreous gel out. A vitrector combines a guillotine style cutting mechanism with vacuum suction. When suction is initiated, the vitreous gel is drawn through a port in the probe tip and then severed by the cutting mechanism. In addition, saline is infused into the eyeball to keep the eyeball distended for treatment. After removing the vitreous gel, the surgeon may treat the retina with a laser (photocoagulation), cut or remove fibrous or scar tissue from the retina, flatten areas where the retina has become detached, or repair tears or holes in the retina or macula. At the end of the surgery, saline, silicone oil, or a gas is injected into the eye to replace the vitreous gel and restore normal pressure in the eye.

Vitrectomies are typically conducted in facilities dedicated to surgical procedures, such as an operating room in a hospital. Special power and gas systems are generally available in such environments. These systems are usually monitored by various computerized alarm systems. In particular, hospitals employ highly controlled power systems that provide uninterrupted electricity throughout the hospital. Furthermore, hospitals employ piped gas systems that supply pressurized oxygen, nitrous oxide, nitrogen, carbon dioxide, and/or clean outside air via pipes to operating rooms and other parts of the hospital. Because vitrectomies are typically conducted in hospital facilities, conventional vitrectomy systems are designed to rely on the special power and gas systems available in such facilities. For example, conventional vitrectomy systems that employ gas-driven vitrectors can be simply connected to a gas port readily available in a hospital operating room to receive the pressurized gas needed for driving the vitrector. Accordingly, conventional vitrectomy systems can-

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not be easily implemented in facilities without special systems that effectively provide unlimited power and pressurized gas.

SUMMARY OF THE INVENTION

In view of the foregoing, aspects of the present invention provide systems and methods that allow vitrectomy to be conducted in a wide variety of clinical environments. Advantageously, embodiments according to aspects of the present invention do not rely on special power and gas systems that are typically only available in special hospital facilities. Thus, such embodiments may be implemented in doctors' offices, which may not have access to special systems that provide power and/or gas.

For example, aspects of the present invention use gas more efficiently so that the vitrectomy system can use widely available and smaller gas cylinders. According to one embodiment, a system for conducting a vitrectomy includes: a gas source; a vitrector including a cutting mechanism that opens and closes according to a pressure at the vitrector; and a pulse-generating system receiving gas from the gas source and generating pulses at the vitrector. The pulses cause the pressure at the vitrector to vary according to a cycle, and the varying pressure at the vitrector causes the cutting mechanism of the vitrector to open and close. At a first time in the cycle, the pulse-generating system raises the pressure at the vitrector to a maximum pressure. At a second time in the cycle, the pulse-generating system reduces the pressure at the vitrector to a minimum pressure that is greater than ambient, the pressure at the vitrector being maintained at least at the minimum pressure. By employing a minimum pressure greater than ambient, the difference between the maximum pressure and minimum pressure is minimized to reduce gas consumption.

Correspondingly, a method for vitrectomy includes: providing a pulse-generating system with gas from a gas source; and generating pulses from the pulse-generating system at a vitrector. The vitrector includes a cutting mechanism. The pulses cause the pressure at the vitrector to vary according to a cycle, and the varying pressure at the vitrector causes the cutting mechanism of the vitrector to open and close. The act of generating pulses includes: raising, at a first time in the cycle, the pressure at the vitrector to a maximum pressure, and reducing, at a second time in the cycle, the pressure at the vitrector to a minimum pressure that is greater than ambient, the pressure at the vitrector being maintained at least at the minimum pressure.

Additional aspects of the invention will be apparent to those of ordinary skill in the art in view of the detailed description of various embodiments, which is made with reference to the drawings, a brief description of which is provided below.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 illustrates an example vitrectomy system according to aspects of the present invention.

FIG. 2 illustrates pneumatics for an example vitrectomy system according to aspects of the present invention.

FIG. 3A illustrates an example of how a vitrectomy system may drive a vitrector according to aspects of the present invention.

FIG. 3B illustrates another example of how a vitrectomy system may drive a vitrector according to aspects of the present invention.

FIG. 4 illustrates aspects of a cut cycle corresponding to the example of FIG. 3A.

FIG. 5 illustrates example electronics corresponding to the example of FIG. 3A.

FIG. 6 illustrates an example of how a vitrectomy system may control aspiration according to aspects of the present invention.

FIG. 7 illustrates example electronics corresponding to the example of FIG. 6.

FIG. 8 illustrates additional example electronics corresponding to the example of FIG. 6.

FIG. 9 illustrates an example of how a vitrectomy system may control the air exchange according to aspects of the present invention.

FIG. 10 illustrates an example power supply for a vitrectomy system according to aspects of the present invention.

FIG. 11 illustrates an example sensing system for a vial of an aspiration cassette in a vitrectomy system according to aspects of the present invention.

FIG. 12A illustrates an example illumination system in a vitrectomy system according to aspects of the present invention.

FIG. 12B illustrates the relative spectral output of an LED in the example illumination system of FIG. 12A.

FIG. 12C illustrates the relative spectral output of filtered LED light in the example illumination system of FIG. 12A.

DETAILED DESCRIPTION

Aspects of the present invention provide systems and methods that allow vitrectomy to be conducted in a wide variety of clinical environments. Advantageously, embodiments according to aspects of the present invention do not rely on special power and gas systems that are typically only available in special hospital facilities. Thus, such embodiments may be implemented in doctors' offices, which may not have access to special systems that provide unlimited power and/or gas.

Aspects of the present invention provide systems and methods for driving a vitrector, providing aspiration, and/or handling fluid-air exchange in a vitrectomy system. Referring to FIG. 1, an example vitrectomy system 100 is illustrated. Components of the vitrectomy system 100 are assembled into an apparatus defined by a housing 102. As shown in FIG. 1, the housing 102 includes a handle 104 to make the vitrectomy system 100 more easily portable. Advantageously, the vitrectomy system 100 is sized for portability and is not restricted to a particular location or facility. For example, the housing 102 may be approximately 0.25 m (10 inches) in width by approximately 0.23 m (9 inches) in height by approximately 0.23 m (9 inches) in depth, and may weigh approximately 5.5 kg (12 lbs).

Operator controls 106, such as adjustable knobs, buttons, switches, and the like, are provided on the exterior of the housing 102. As described below, the operator controls 106 control aspects of the vitrectomy system 100, such as the cut speed of the vitrector, the level of aspiration, amount of illumination, etc.

In addition, a vitrector connection 108, e.g., a luer connection, is provided on the exterior of the housing 102 to removably couple a vitrector to the components in the housing 102. An air exchange connection 110, e.g., a luer connection, is also provided on the exterior of the housing 102 to removably couple an air exchange tubing set to the components in the housing 102. Additionally, an aspiration cassette 111 is removably received in a cassette receptacle 103 defined by the housing 102 and coupled to the components in the housing

102, e.g., via a luer. As described further below, the aspiration cassette 111 provides aspiration vacuum via an aspiration cassette connection 109 and receives aspirated vitreous gel and saline. Furthermore, a gas source 112 is removably coupled via a gas source connector to the components in the housing 102.

Referring to FIG. 2, example pneumatics for the vitrectomy system 100 are illustrated. The vitrectomy system 100 pneumatically drives a low-pressure gas-driven vitrector 210. An operator of the vitrectomy system 100 activates a cut/aspirate mode via the controls 106 to operate the vitrector 210. The gas source 112 provides input gas for driving the vitrector 210. The input gas is regulated at the gas source 112 to a lower input pressure, e.g., approximately 80 psig, which is monitored by a pressure transducer 204.

A pulse-generating system 206 receives the gas from the gas source 112 and generates pulses of gas pressure that drive the vitrector 210. The gas pressure in the pulse-generating system 206 is further regulated to a lower pressure, e.g., approximately 16 psig. The pulses of gas cause a cutting mechanism of the vitrector 210 to open and close according to a cycle. The open/close action of the cutting mechanism cuts the vitreous gel when the vitrector 210 is applied to the eye. The rate at which the pulse-generating system 206 produces the pulses of gas depends on a cut speed the operator selects for the vitrector 210 via the controls 106. In some embodiments, for example, the cut speed may be selected from a range of approximately 60 cuts per minute (cpm) to approximately 2500 cpm.

Vitrector tubing 208 extends between the vitrector connection 108 shown in FIG. 1 and the vitrector 210. The vitrector tubing 208 includes a first tube 208a. The vitrector connection 108 couples the first tube 208a to the pulse-generating system 206 disposed at the housing 102. The first tube 208a carries the pressure pulses from the pulse-generating system 206 to the vitrector 210.

The vitrector tubing 208 also includes a second tube 208b. The aspiration cassette connection 109 couples the second tube 208b to the aspiration cassette 111 disposed in the recess 103. The second tube 208b provides a vacuum to the vitrector 210. The aspiration cassette 111 is removably coupled to a vacuum source 222 and collects aspirant received from the vitrector 210 via the second tube 208b.

The vitrector tubing 208, for example, may include twin-bore PVC tubing having a length of approximately 1 m to approximately 2 m. For a length of approximately 1 m, each tube 208a, b may have an inner diameter of approximately 0.81 mm (0.032 inches) and an outer diameter of approximately 2.4 mm (0.094 inches). For a length of approximately 2 m, each tube 208a, b may have an inner diameter of approximately 1.6 mm (0.062 inches) and an outer diameter of approximately 3.2 mm (0.125 inches). The tubing length is determined in part by the desired distance between a patient and the housing 102. In other words, the tubing length should allow the operator to extend the vitrector 210 to a patient positioned suitably away from the housing 102. In addition, the tubing length should provide sufficient slack so that the operator can manipulate the vitrector 210 in space without significant restriction.

The vitrector tubing 208 may be selected from an array of standard-sized tubing formed from medical grade materials. Specifically, from the array of choices, tubing of varying lengths, inner diameters, outer diameters, and durometers may be evaluated for their performance for various configurations of components, e.g., pneumatic components, for the vitrectomy system 100. The vitrector tubing 108 provides sufficient gas flow to drive the vitrector 210 at the required cut

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speeds. The highest cut speed requires the highest gas flow in the vitrector tubing 208 leading to the vitrector 210.

The gas source 112 also provides input gas for driving a pinch valve drive 212. The pinch valve drive 212 in turn operates a pinch valve 218 which controls aspiration from the eye during the procedure. An air cylinder of the pinch valve 218 closes the second tube 208b of the vitrector tubing 208 to block flow. To allow aspiration through the second tube 208b, pressure is applied to the pinch valve 218 which causes the air cylinder to retract. Pressure is applied to the pinch valve 218 when the cut/aspirate mode is activated or when the aspiration cassette 111 is missing. When the cut/aspirate mode is deactivated, the pressure is relieved from the pinch valve 218 causing the pinch valve 218 to pinch and close the second tube 208b. When the cut/aspirate mode is deactivated, closure of the pinch valve 218 is delayed to allow the second tube 208b to vent to atmosphere. In some embodiments, the pinch valve 218 pinches the second tube 208b against a surface of the aspiration cassette 111.

As described previously, the aspiration cassette 111 is coupled to the second tube 208b of the vitrector tubing 208 and the vacuum source 222. The vacuum in the aspiration cassette 111 from the vacuum source 222 draws aspirant from the vitrector 210 via the second tube 208b to a vial in the aspiration cassette 111. The vacuum level in the aspiration cassette 111 and the level of aspiration are controlled by an adjustable vacuum control 221 provided with the controls 106. When the cut/aspirate mode is deactivated, closure of the pinch valve 218 is delayed also to allow the aspiration cassette 111 to vent to atmosphere. When the pinch valve 218 closes, the vacuum in the aspiration cassette 111 returns to the level determined by the vacuum control 221. The vacuum level of the aspiration cassette 111 is monitored with a pressure transducer 228. In operation, the aspiration cassette 111 may be positioned substantially level with the patient's eye, thereby minimizing aspiration perturbations caused by the fluid column between the aspiration cassette 111 and the eye.

The vial of the aspiration cassette 111, for example, may have a volume of approximately 25 cc. The volume of aspirant received in the vial may be monitored with a sensor system 1100 shown in FIG. 11. In addition to detecting whether a vial contains a threshold volume of aspirant, the sensor system 1100 also detects whether the aspiration cassette 111 is missing from the vitrectomy system 100. The sensor system 1100 includes a pair of infrared light emitting diodes (LED's) 1104a, b that are arranged to project two separate infrared beams through the vial. A pair of transistors 1106a, b are correspondingly positioned to receive the infrared beams projected through the vial. When the aspiration cassette 111 is missing from the vitrectomy system 100, the infrared beams do not pass through the vial and thus experience substantially no scatter. Because there is substantially no scatter, the infrared energy reaching the transistors 1106a, b is substantially equal to the maximum. A CASSETTE MISSING threshold corresponding to this maximum level of infrared energy is set. When both of the transistors 1106a, b receive infrared energy that is greater than the CASSETTE MISSING threshold, the aspiration cassette 111 is considered to be missing.

When the aspiration cassette 111 is installed and present in the vitrectomy system 200, the infrared beams experience some scatter due to the vial and the amount of infrared energy reaching the transistors 1106a, b is reduced to a level below the CASSETTE MISSING threshold. As the aspirant fills the vial, the LED's 1104a, b are positioned so that the infrared beams have to pass through the aspirant when the vial becomes substantially full with aspirant. When the infrared

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beams pass through the aspirant, the infrared beams experience additional scattering and the infrared energy reaching the transistors 1106a, b is reduced further. A CASSETTE FULL threshold corresponding to this reduced level of energy is determined. When either transistor 1106a, b receives infrared energy lower than the CASSETTE FULL threshold, the vial is considered to be full. In general, the strength of the signal received by the transistors 1106a, b indicates whether aspiration cassette 111 is not present in the vitrectomy system 100 or whether the volume of aspirant has reached a certain volume. After the vitrectomy system 100 detects that the vial is full, the vitrectomy system 100 may be reset when it detects that the aspiration cassette 200 has been removed, or when the vitrectomy system 100 is reset by a POWER/RESET function via the controls 106.

Referring again to FIG. 2, the vitrectomy system 200 generates a vacuum internally via the vacuum source 222. The maximum vacuum, for example, may be approximately 500 mm Hg to approximately 700 mm Hg (at sea level). The vacuum source 222 does not operate if the vitrectomy system 100 is stopped due to a detected error condition, e.g., if there is a problem with the input gas pressure or the battery charge level or if the aspiration cassette 111 is missing.

The vacuum source 222 is coupled to a vacuum accumulator 224. The vacuum accumulator 224 stores system vacuum and has the capacity to maintain vacuum in the aspiration cassette 111 even when the vacuum source 222 is not operating. The accumulator, for example, may have a volume of approximately 250 cc. The vacuum accumulator 224 also smoothes variations when the vacuum source 222 is operating. The vacuum level in the vacuum accumulator 224 is monitored with a pressure transducer 226.

The vitrectomy system 100 generates low pressure air internally via a pressure source 230 to provide air exchange. The air exchange controls infusion pressure of an infusion fluid by adjusting a pressure in an irrigation bottle during the procedure. The air exchange may also deliver low pressure air to the eye during an air-fluid exchange. The low pressure air is directed to an accumulator 232. The accumulator 232 stores pressure, e.g., at approximately 5 psig. The accumulator 232 also smoothes variations when the pressure source 230 is operating. Once the low pressure source 230 provides the required pressure in the accumulator 232, the accumulator 232 has the capacity to allow the pressure source 230 to be implemented as a supplemental vacuum source. The output pressure from the pressure source 230 is determined by an air exchange control 234 provided with the controls 106. The air exchange may be maintained regardless of whether the cut/aspirate mode is activated or deactivated or whether there are error conditions. Advantageously, the internal generation of low pressure air allows the vitrectomy system 100 to operate independently of any special external air pressure source.

In one embodiment, an irrigation fluid bottle containing saline is connected to the air exchange connection 110 via an air exchange tube set. The air exchange tube set is a PVC tubing set intended to deliver forced air or fluid during ophthalmic surgery. The air exchange tube set includes a three channel IV spike for insertion into the bottle. The three-way spike is designed to deliver air from the pressure source 230 through the saline, while the dual PVC tubing administers air and saline. The dual PVC tubing has a three-way stopcock for proper connection. The irrigation fluid bottle may be positioned so that it is substantially level with the eye. The spike from the air exchange tube set is coupled to the bottle and an infusion cannula is coupled to the other end of the air exchange tube set. The air exchange control 234 is set to provide a desired infusion pressure.

FIGS. 3A-B, 4, and 5 illustrate examples of how the vitrectomy system 100 may drive the vitrector 210 and control the pinch valve 218. The gas pressure source 112, for instance, includes a conventional tank 312a containing carbon dioxide (CO₂) at a pressure of approximately 900 psig. The gas tank 312a is removably received by the housing 102 and screwed to a gas source connector until it is firmly seated.

Employing a conventional tank to supply gas to the vitrectomy system 100 allows the vitrectomy system 100 to be operated without access to a special gas supply system typically available in special hospital facilities. The vitrectomy system 100, for example, may accept gas cylinders ranging in size from 12 g to 33 g. The size of such gas cylinders enhances the portability of the vitrectomy system 100. Moreover, compatibility with standard smaller off-the-shelf gas tanks enhances the convenience and cost effectiveness of using the vitrectomy system 100. Additionally, the smaller size and relatively lower cost of the gas cylinder allows it to be included in a convenient disposable package that is used for each procedure.

The pressure in the gas tank 312a is regulated, e.g., to a pressure of approximately 80 psig, using a tank-mounted high pressure regulator 312b. Protection from liquid CO₂ intrusion into the high pressure regulator 312b is provided by an adapter between the gas source connector and the high pressure regulator 312b. The pressure transducer 204 is used to monitor the output from the high pressure regulator 312b. If the pressure drops below a minimum threshold, e.g., 70 psig, the vitrectomy system 100 shuts off.

The low pressure regulator 313 reduces the gas pressure, e.g., to approximately 16 psig. The pulse-generating system 206 includes a valve combination 314. The gas from the low pressure regulator 313 is directed to the valve combination 314 to generate pressure pulses for driving the vitrector 210. The pressure pulses cause the pressure at the vitrector 210 to vary according to a cycle, and the varying pressure at the vitrector 210 causes the cutting mechanism of the vitrector 210 to open and close.

As shown in the example embodiment of FIG. 3A, the valve combination 314 may include a two-way pressurize valve 314a and a two-way exhaust valve 314b. The pressurize valve 314a is coupled to the low pressure regulator 313 and to the vitrector 210. At the beginning of a cut cycle, the pressurize valve 314a opens for approximately 6 ms to raise the pressure to a maximum of approximately 14 psig at the vitrector 210. A pressure curve 400 shown in FIG. 4 illustrates the pressure at the vitrector 210 during the cut cycle as a function of time. A corresponding curve 410 shown in FIG. 4 indicates when the pressurize valve 314a remains open during a period 412 in the cut cycle. The maximum pressure is shown as peak 402.

The exhaust valve 314b is coupled to the vitrector 210 and to atmosphere through a muffler. During the cut cycle, the exhaust valve 314b opens for approximately 18 ms to reduce the pressure at the vitrector 210 from the maximum pressure to a minimum pressure of approximately 4 psig. A curve 420 shown in FIG. 4 indicates when the exhaust valve 314b remains open during a period 422 in the cut cycle. Taken together the curves 400, 410, and 420 illustrate how the pressure at the vitrector 210 responds to the opening/closing of the pressurize valve 314a and the opening/closing of the exhaust valve 314b. The minimum pressure is shown in pressure curve 400 of FIG. 4 as trough 404. As illustrated in FIG. 4, the opening and closing of the valves 314a, b are timed to achieve a desired pressure profile, e.g., the pressure curve 400. With certain types of valves, the time and manner in which the valves 314a, b open may be different from the time

and manner in which the valves 314a, b close. Thus, to account for this asymmetric behavior in FIG. 4, for example, there is a delay of approximately 8 ms between the time when the pressurize valve 314a is closed and the time when the exhaust valve 314b is opened.

Alternatively, as shown in the embodiment of FIG. 3B, the valve combination 314 includes a three-way pressurize valve 314c and a two-way exhaust valve 314d. The pressurize valve 314c is coupled to the low pressure regulator 313, the vitrector 210, and the exhaust valve 314d. The two-way valve 314d is coupled to the pressurize valve 314c and to atmosphere through a muffler. At the beginning of the cut cycle, the pressurize valve 314a opens for approximately 6 ms to raise the pressure to a maximum of approximately 14 psig at the vitrector 210. When the pressurize valve 314c closes, the vitrector 210 is coupled to the exhaust valve 314d via the pressurize valve 314c. Thus, the exhaust valve 314d opens at the same time that the pressurize valve 314c closes. The exhaust valve 314d couples the vitrector 210 to atmosphere via a muffler. The exhaust valve 314d remains open for approximately 18 ms and reduces the pressure at the vitrector 210 from the maximum to a minimum of approximately 4 psig.

In general, the embodiments of the pulse-generating system 206 shown in FIGS. 3A-B include a first valve and a second valve, where the first valve and the second valve are operable to raise and reduce the pressure at the vitrector 210 according to a cycle that drives the vitrector 210. At a first time in the cycle, the pulse-generating system 206 raises the pressure at the vitrector 210 to a maximum pressure. At a second time in the cycle, the pulse-generating system 206 reduces the pressure at the vitrector 210 to a minimum pressure that is greater than ambient. Instead of exhausting the gas from the vitrector 210 and in the vitrector tubing 208 until the pressure reaches ambient, the pressure at the vitrector 210 and in the vitrector tubing 208 is maintained at a minimum pressure that is greater than ambient. As a result, to raise the pressure to the maximum pressure during the cut cycle, the gas source 112 is required to supply less gas than would otherwise be required if the pressure at the vitrector 210 and in the vitrector tubing 108 were permitted to drop to ambient. Accordingly, the embodiments use gas more efficiently during the cut cycle and deplete the supply gas from the gas source 112 more slowly.

The efficient use of gas by the vitrectomy system 100 is particularly advantageous if the vitrectomy system is employed with gas tanks that are 12 g to 33 g in size, for example. The embodiments shown in 3A-B can provide approximately 6 minutes to approximately 19 minutes of vitrector operation when gas pressure in the system is kept at or above a minimum threshold greater than ambient. The operating time depends on the cut speed of the vitrector 210. For example, a 16 g cylinder tank may provide approximately 8 to approximately 9 minutes of vitrector operation when the vitrector 210 is operated at 1200 cpm. Of course, in some embodiments, an adapter is available to allow the vitrectomy system 100 to be used with a special gas supply system, if available. The special gas supply system effectively extends the operating time of the vitrectomy system 100 indefinitely.

Although the embodiments described previously raise the pressure to a maximum of approximately 14 psig at the vitrector 210 and reduce the pressure to a minimum pressure of approximately 4 psig, the maximum and minimum pressures during the cut cycle may be different in other embodiments. The maximum and minimum pressures are selected according to the pressures required to operate the vitrector 210. For instance, the maximum pressure during the cut cycle should

be sufficient to cause the cutting mechanism of the vitrector **210** to close completely and to achieve the required cut speed. Higher cutting speeds can be achieved with greater spring force in the cutting mechanism of the vitrector **210** and correspondingly higher applied pressure. To promote efficient use of gas, the maximum pressure is preferably the lowest pressure required for the cutting mechanism to close completely. The pressure required for the cutting mechanism to close completely depends partially on the force required to overcome the friction as well as the spring force associated with the cutting mechanism of the vitrector **210**.

Meanwhile, the minimum pressure during the cut cycle should be sufficiently low to cause the cutting mechanism to open completely. To promote efficient use of gas further, the minimum pressure is preferably the highest possible pressure that still ensures that the cutting mechanism of the vitrector **210** opens completely. In general, embodiments employing the valve combination **314** described above achieve more efficient use of gas by minimizing the difference between the maximum and minimum pressures during the cut cycle. In some embodiments, the greatest efficiencies are achieved with a pressure difference of approximately 8 psig to approximately 10 psig.

The pressurize valve and the exhaust valve are opened for the necessary periods of time to achieve a maximum pressure and a minimum pressure, respectively. The periods of time, as well as the minimum and maximum pressures, depend on the structure and configuration of the valve combination **314** and the vitrector **210**. Typically, the pressurize valve does not remain open longer than half the time for the cut cycle, because it takes more time for the exhaust valve to reduce the pressure to the minimum than it takes for the pressurize valve to raise the pressure to the maximum. To optimize air flow in the vitrectomy system **100**, the pulse-generating system **206** may be adjusted to deliver a maximum pressure that is sufficient to provide the largest cut speed during the shortest amount of time required to open the pressurize valve.

In addition to achieving more efficient use of gas and extending the operating time provided by the gas source **112**, it has been discovered that embodiments that minimize the difference between the maximum and minimum pressures during the cut cycle also provide additional advantages. In particular, the embodiments reduce the noise associated with operating the vitrectomy system **100**. Noise is a distraction during the procedure. Conventionally, mufflers are used in vitrectomy systems to reduce noise, but the noise is generally difficult to muffle due to the pulsing nature of the vitrectomy system **100**. Changing the minimum and maximum pressures as described above, however, yields greater noise reduction, because less air is being moved during each cut cycle.

Furthermore, the embodiments also reduce the amount of stiffness that the gas pressure causes in the vitrector tubing **208**. The stiffness increases with greater average operation pressure in the vitrector tubing **208**. The vitrector **210**, however, is easier to manipulate when the vitrector tubing **208** remains more flexible.

In addition, when the difference between the maximum and minimum pressures is larger and the vitrector tubing **208** is stiffer, the vitrector tubing **208** has a greater tendency to bounce or vibrate and transfer disturbances to the operator's hand holding the vitrector **210**. Accordingly, reducing the stiffness of the vitrector tubing **208** gives operators a greater tactile feel and steadier control of the vitrector **210**.

As discussed previously, the vitrector tubing **108** must provide sufficient gas flow to drive the vitrector **210** at the required cut speeds. The vitrectomy system **100**, however, also minimizes consumption of the gas from the gas source

112. A longer tube with larger inner diameter provides a higher gas flow rate and results in more gas consumption. Conversely, a shorter tube with smaller inner diameter provides a lower gas flow rate and results in less gas consumption. As discussed previously, the length of the vitrector tubing **208** is determined by practical considerations. For example, the length of the vitrector tubing **208** is not shorter than 1 meter. Thus, for a given length of the vitrector tubing **208**, the inner diameter may be reduced to the point where the gas flow cannot drive the vitrector **210** at the required cut speeds. In addition to minimizing gas consumption, the smaller inner diameter results in less stiffness in the vitrector tubing **210**.

Referring again to FIG. 3B, the pinch valve drive **212** also employs a valve combination **322** to control the pressure that drives the pinch valve **218**. The valve combination **322** includes a pressurize valve **322a** and an exhaust valve **322b**. The pressurize valve **322a** is connected to the low pressure regulator **313** and an air cylinder for the pinch valve **218**. The air cylinder of the pinch valve **218** may be a reverse acting (spring extended) air cylinder that aids in closing the second (aspiration) tube **208b** of the vitrector tubing **208**. In operation, the pressurize valve **322a** opens, e.g., for approximately 100 ms, to open the pinch valve **218**. The exhaust valve **322b** is connected to the air cylinder of the pinch valve **218** and to atmosphere through a muffler. The exhaust valve **322b** opens, e.g., for approximately 100 ms, to close the pinch valve **218**.

FIG. 5 illustrates example electronics for driving the vitrector **210** and controlling the pinch valve **218** for a vitrectomy system **100** that employs the valve combination **314** shown in FIG. 3A. The vitrector **210** is controlled by an illuminated toggle switch **502** and an adjustable potentiometer **522** provided with the controls **106**. The adjustable potentiometer **522** determines the cut rate for the vitrector **210**. The switch **502** is operated to alternate between activating and deactivating the cut/aspirate mode and to respectively enable or disable cutting with the vitrector **210**. When the cut/aspirate mode is deactivated, the aspiration system is also returned to atmosphere with the pinch valve **218** closed. The switch **502** is illuminated with a combination RED/GREEN LED **504**. The LED is illuminated RED when the available gas pressure falls below a minimum threshold, e.g., approximately 70 psig. The LED is illuminated GREEN when the cut/aspirate mode is activated. The LED is not illuminated when the cut/aspirate mode is deactivated.

Operation of the vitrectomy system **100** is enabled when the switch **502** is switched to activate the cut/aspirate mode. Although embodiments of the vitrectomy system **100** may employ a microprocessor, the embodiment shown in FIG. 5 employs discrete integrated circuit (IC) functional blocks (logic gates, flip-flops, multivibrators, etc.). In particular, the vitrectomy system **100** employs a multivibrator chain **506** that determines operation of the vitrector **210** according to the cut cycle. Thus, when the switch **502** is switched to ON, the switch pull-up resistor **504** is grounded and the RESET signal is removed from the multivibrator chain **506**. The monostable multivibrator **506a** is triggered to open the two-way pressurize valve **314a**. Triggering the monostable multivibrator **506a** causes the pressure to increase at the vitrector **210** and the cutting mechanism to close. After the pressurize valve **314a** is closed for the required amount of time, e.g., approximately 6 ms, the next monostable multivibrator **506b** is triggered. As described previously, there is a delay, e.g., approximately 8 ms, between the time when the pressurize valve **314a** is closed and the time when the exhaust valve **314b** is opened. After the delay time expires, the final monostable multivibrator **506c** in the chain **506** is triggered. The monostable mul-

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tivibrator **506c** opens the two-way exhaust valve **314b** and causes the cutting mechanism of the vitrector **210** to open. The exhaust valve **314b** closes after the required amount of time, e.g., approximately 18 ms. When the cut/aspirate mode is activated with the switch **502**, an astable multivibrator **506d** runs at the cut rate selected for the vitrector **210**. The astable multivibrator **506d** triggers the monostable multivibrator **506a** controlling the pressurize valve **314a** and repeats the cut cycle.

During the procedure, the tip of the vitrector **210** is placed at an area of vitreous gel requiring removal. The cut/aspirate mode may be activated through the toggle switch **502** or a foot pedal. When the cut/aspirate mode is activated, the vitrectomy system **100** cuts and aspirates at the levels determined by the adjustable cut rate control **522** and the adjustable vacuum control **221**. Once the desired volume of vitreous gel has been removed, the cut/aspirate mode is deactivated by pressing the toggle switch **502** again or by releasing the foot pedal.

When the cut/aspirate mode is deactivated, the cutting mechanism of the vitrector **210** stops immediately. In addition, the monostable multivibrator **506c** controlling the exhaust valve **314b** is triggered to force the cutting mechanism of the vitrector **210** to open.

FIG. 6 illustrates an example of how the vitrectomy system **100** may control aspiration. The vacuum source **222** includes a vacuum pump **602**, such as a 6 VDC diaphragm pump. The exhaust for the vacuum pump **602** is connected to a muffler. The vacuum pump **602** is activated when the vacuum at the vacuum accumulator **224** drops below a vacuum pressure activation threshold. The vacuum pressure activation threshold, for example, is set to a pressure approximately 25 mmHg above the aspiration level specified by the adjustable vacuum control **221**. The vacuum level in the vacuum accumulator **224** is monitored with a pressure transducer **226**. As shown in the electronics of FIG. 7, a vacuum level determined by a sensor **702** is compared to the vacuum pressure activation threshold. The vacuum level determined by the sensor **702** is also compared to a vacuum pressure deactivation threshold. The vacuum pump **702** is stopped when the vacuum in the accumulator meets the vacuum pressure deactivation threshold (or when an error condition occurs).

As illustrated further in FIG. 6, a proportional valve **612a** and a two-way valve **612b** control the vacuum level in the aspiration cassette **111**. The proportional valve **612a** is coupled to the vacuum accumulator **224** and the aspiration cassette **111** (through a hydrophobic filter **616**). The proportional valve **612** is operated to lower the pressure in the aspiration cassette **111** to the value determined by the vacuum control **221**. The proportional valve **612a** is opened by an amount that minimizes overshoot and vacuum response time. The vacuum level of the aspiration cassette **620** is monitored with a pressure transducer **228**. The two-way valve **612b** is coupled to the aspiration cassette **111** and to atmosphere. The two-way valve **612b** is operated to raise the pressure in the aspiration cassette **111**.

FIG. 8 illustrates example electronics for controlling the aspiration in the vitrectomy system **100**. The operator controls the aspiration level by the adjustable vacuum control **221**, which includes a potentiometer **802** or a linear foot pedal **804**. The adjustment allows the vacuum to be set, for example, from approximately 25 mmHg to approximately 500 mmHg. The setting is compared with a vacuum sensor **806** that is coupled to the aspiration cassette **111**. The vacuum sensor **806** may be similar to the sensor **702** that monitors the

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vacuum of the vacuum accumulator **224**. In both cases, the sensors have a 4 VDC range which equates to 15 psig (approximately 775.7 mmHg).

If the vacuum level in the aspiration cassette **111** is less than the aspiration level set by the operator (and there is no error condition or cassette venting in progress), the two-way valve **612a** opens and couples the aspiration cassette **111** to the vacuum accumulator **224**. The aspiration cassette **111** passes air to the vacuum accumulator **224** causing a reduction of pressure in the aspiration cassette **111**. Once the vacuum level in the aspiration cassette **111** matches the aspiration level set by the user, the two-way valve **612a** closes and decouples the aspiration cassette **111** from the vacuum accumulator **224**.

The aspiration cassette **111** is coupled to atmosphere when the vacuum level in the aspiration cassette **111** is higher than an aspiration cassette vacuum threshold. If the vacuum level in the aspiration cassette **111** is greater than the aspiration cassette vacuum threshold or venting of the aspiration cassette **111** is in progress, the two-way valve **612b** allows the aspiration cassette **111** to attain atmospheric pressure.

A second mechanism controls venting of the aspiration cassette **111** to atmosphere when the cut/aspirate mode is deactivated or an alarm condition occurs. In this case, a D latch causes the proportional valve **612a** to close the connection between the aspiration cassette **111** and the vacuum accumulator **224**, while the two-way valve **612b** connects the aspiration cassette **111** to atmosphere. Once the aspiration cassette **111** meets the CASSETTE AT ATMOSPHERE threshold, the D latch is reset and the pinch valve **218** pinches the tube **208b** closed. Resetting of the D latch also allows the proportional valve **612a** to couple the aspiration cassette **111** to the vacuum accumulator **224** so that the aspiration cassette **111** can be driven subsequently to the vacuum level set by the operator.

The pinch valve **218** is opened for normal aspiration when the cut/aspirate mode is activated (and no error conditions are present). The pinch valve **218** is also opened if the aspiration cassette **111** is removed from the vitrectomy system **100** to install a replacement cassette.

FIG. 9 illustrates an example of how the vitrectomy system **100** may handle air exchange. The pressure source **230** includes a pressure/vacuum pump **902**, such as a 6 VDC diaphragm pump. Through two three-way valves **904a, b**, the pressure/vacuum pump **902** can be employed for air exchange function as well as aspiration function. The three-way valves **904a, b** are configured so that when they are closed, the pressure/vacuum pump **902** delivers pressure for air exchange function. Conversely, when the three-way valves **904a, b** are open, the pressure/vacuum pump **902** delivers vacuum for aspiration function. Priority is given to the air exchange function. The pressure/vacuum pump **902** is operated to increase the pressure at the accumulator **232** when the pressure drops below a threshold, e.g., approximately 5 psig. The pressure at the accumulator **232** is monitored with the pressure transducer **236**.

As FIG. 9 illustrates further, a proportional valve **912a** and a two-way valve **912b** are employed to control the output level of the air exchange pressure. The proportional valve **912a** is coupled to the accumulator **232** and the output **110** (through a hydrophobic filter). The proportional valve **912a** is operated to raise the output pressure to the value set by the air exchange control **234**. Once the output pressure reaches the set value, the proportional valve **912a** is closed or its opening is adjusted to match a constant flow load. The amount that the proportional valve **912a** opens is controlled to minimize overshoot and pressure response time. The output pressure level is

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monitored by a pressure transducer **916**. Meanwhile, the two-way valve **912b** is coupled to the output **914** and to atmosphere and is operated to lower the output pressure.

Referring to FIG. **10**, the vitrectomy system **100** employs a rechargeable battery **1002**. The vitrectomy system **100** can be coupled to an external power source to recharge the rechargeable battery **1002**. It is not necessary, however, for the vitrectomy system **100** to be completely charged to use it. When connected to the external power source, the vitrectomy system **100** operates with the power from the external power source while the rechargeable battery **1002** is recharged. Advantageously, the rechargeable battery **1002** allows the vitrectomy system **100** to be operated without access to an external power source. The rechargeable battery **1002** enhances the portability of the vitrectomy system **100**. Moreover, the rechargeable battery **1002** can be conveniently recharged by connecting the vitrectomy system to a conventional electrical wall socket.

It is also not necessary to turn on the vitrectomy system **100** for the battery **1002** to charge. If the vitrectomy system **100**, however, is turned on, a power indicator shows the state of battery charge. The power indicator illuminates via a GREEN and a RED LED. If the power indicator illuminates RED, there may not be enough charge to complete the procedure. In some cases, the power indicator may not illuminate due to a depleted battery **1002**. Three comparators **1004a-c** are utilized to provide a visual indication of the battery run time. The first comparator **1004a** determines whether the estimated battery run time exceeds 30 minutes. The second comparator **1004b** determines whether the estimated battery run time exceeds 20 minutes. These two comparator outputs pass through a transparent latch **1006** that is enabled when the vitrectomy system **100** is operating from the rechargeable battery **1002**, and is selectively enabled during certain periods as the rechargeable battery **1002** is charging. The outputs from the latch **1006** are coupled to an astable multivibrator **1008** that is forced into reset when the battery voltage exceeds 30 minutes (GREEN power indicator) and is forced into trigger when the battery voltage falls below 20 minutes (RED power indicator). Between 20 minutes and 30 minutes, the multivibrator **1008** is allowed to run at a 60 Hz rate (combining RED and GREEN to provide a YELLOW power indicator). The third comparator **1004c** determines whether the estimated battery run time is less than 3 minutes, in which case an alarm is provided to alert the operator.

While some components of the vitrectomy system **100** may be reusable, other components, such as the gas cylinder tank **202a**, the vitrector **210**, the vitrector tubing **208**, the aspiration cassette **111**, irrigation tubing, etc., may be disposable and provided for use in a single procedure. The disposable components may be conveniently packaged in a single disposable pack, e.g., with Tyvek® material. The vitrector **210**, the vitrector tubing **208**, the aspiration cassette **111**, and the irrigation tubing are disposed in a manner consistent with other contaminated waste.

The vitrectomy system **100** may also include a disposable endoilluminator. The illumination level may be adjusted to a desired amount with the controls **106**. The light output is reduced when a probe of the endoilluminator is not in the eye to reduce the possibility of damage to the fibers of the endoilluminator and to increase battery life.

FIG. **12A** illustrates an example illumination system **1200** for providing light to the endoilluminator via an output connector receptacle **1202**. The output connector receptacle accepts an optical fiber connector. In one embodiment, for example, the optical fiber connector may be constructed from a 19-gauge hypodermic needle (approximately 1.1 mm (0.42

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inches) in diameter) having a length of approximately 6.35 cm (2.5 inches). The light source in the illumination system **1200** includes an LED **1205**. As shown in FIG. **12A**, the LED **1205** is provided on a printed circuit board (PCB) **1203**. For example, the LED **1205** may be a blue-violet LED (approximately 435 nm) with a phosphor coating to convert a portion of the light to broadband light of longer wavelength that appears white. The light emitting portion of the LED **1205** may be approximately 2 mm². FIG. **12B** illustrates the relative spectral output of the LED **1205**.

The LED **1205** includes a flat window that protects the diode surface but does not significantly affect the radiation pattern of the LED **1205**. A lens **1206** gathers light from the LED **1205**. The lens **1206**, for example, is a plastic hybrid asphere with a numerical aperture (NA) of 0.63. The lens **1206** has a combination of aspheric and diffractive surfaces to reduce both chromatic and spherical aberration common to traditional lens designs. The light emitting surface of the LED **1205** is placed at the focal point of the lens **1206**. Light exiting the lens **1206** is generally collimated. An absorptive filter **1208** is placed in the light column to tailor the spectral distribution. The filter **1208**, for example, may be formed from Schott GG435 glass that is approximately 6 mm thick. The filter **1208** works in concert with the specific spectral output of the LED **1205**. In other words, the specification for the filter **1208** may depend on the LED output spectrum. Consideration is given to color, phototoxicity, and luminous efficacy of the output spectrum during specification of the filter **1208**. As a reference, the unfiltered output from the LED **1205** may measure 0.30, 0.28 CIE chromaticity, 625 lumens per hazardous watt, and 271 lumens per watt, while the filtered output may measure 0.36, 0.39 CIE chromaticity, 1951 lumens per hazardous watt, and 363 lumens per watt. All of which are much more desirable for an ophthalmic light source. FIG. **12C** illustrates the relative spectral output of the filtered LED light.

A second lens **1210**, which is substantially similar to the collimating lens **1206**, gathers the filtered light and focuses it to an image of the LED **1205**. The proximal end of an optical fiber **1202** is placed at the focal point of the second lens **1210** to guide the light to the surgical field.

Output power from the LED **1205** may be sensitive to temperature. As operating current is increased, die temperature also tends to increase. As die temperature increases, the output light level at a fixed drive current tends to decrease relative to the same drive current at lower temperature. The PCB **1203** to which the LED **1205** is mounted maximizes heat removal from the LED **1205**. The board, for example, may be formed from approximately 0.38 mm (0.015 inch) thick fiberglass with copper traces (for signals and power) located on the top (LED) side of the board. Plated through-holes provide attachment points to solder the PCB **1203** to a copper base plate **1209**, e.g., having a thickness of approximately 3.175 mm (0.125 inch). The copper base plate **1209** has a copper post of approximately 0.38 mm (0.015 inch) that protrudes through a hole in the PCB **1203** to provide direct contact between the central contact of the LED **1205** and the copper base plate **1209**. The central contact of the LED **1205** is provided to allow heat to be conducted away from the light emitting die. This configuration allows the heat from the LED **1205** to quickly spread across a large area with minimal thermal resistance. The copper base plate **1209** is mounted to a Peltier cooler **1207**. The Peltier cooler **1207** pumps heat from the copper base plate **1209** to an aluminum post **1204** to which the cooler **1207** is mounted. The amount of heat that is pumped relates to the amount of drive current given to the Peltier cooler **1207**. The aluminum post **1204** is mounted to a

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multi-finned aluminum heat sink. The heat sink efficiently transfers heat to cooling air that is blown across it by that fan that is also mounted onto the heat sink. A thermistor is mounted on the PCB 1203 with a direct connection to the copper post to monitor LED temperature. Control electronics use the signal from the thermistor to adjust the Peltier cooler 1207 current and control temperature of the LED 1205.

As described above, aspects of the present invention provide systems and methods for driving a vitrector, providing aspiration, and handling fluid-air exchange in a vitrectomy system without relying on special power and gas systems. For example, aspects of the present invention use gas more efficiently so that the vitrectomy system can use widely available and smaller gas cylinders. Thus, corresponding embodiments are portable and may be used in a variety of clinical environments.

While the present invention has been described in connection with a number of exemplary embodiments, and implementations, the present inventions are not so limited, but rather cover various modifications, dimensions, shapes, and equivalent arrangements. Other implementations of the invention will be apparent to those skilled in the art from consideration of the specification and practice of the invention disclosed herein. Various aspects and/or components of the described embodiments may be used singly or in any combination. It is intended that the specification and examples be considered as exemplary only. For example, although embodiments described above may be indicated for vitreous biopsy and vitreous taps, aspects of the present invention may be applied in other procedures, such as float-ectomies and blood removal.

What is claimed is:

1. A system for conducting a vitrectomy, comprising:
 - a gas source;
 - a vitrector including a cutting mechanism that opens and closes according to a pressure and a spring force at the vitrector; and
 - a pulse-generating system receiving gas from the gas source and generating pulses at the vitrector, the pulses causing the pressure at the vitrector to vary according to a cycle, the varying pressure and a spring force at the vitrector causing the cutting mechanism of the vitrector to open and close,
 wherein, at a first time in the cycle, the pulse-generating system, generates a pulse and raises the pressure at the vitrector to a maximum pressure, to close the cutting mechanism, and
 - at a second time in the cycle, the pulse-generating system reduces the pressure at the vitrector to a minimum pressure that is greater than ambient, the pressure at the vitrector being maintained at least at the minimum pressure and the spring force causing the cutting mechanism to open.
2. The system of claim 1, wherein the pulse-generating system includes a first valve and a second valve, the first valve and the second valve being operable to raise and reduce the pressure at the vitrector according to the cycle.
3. The system of claim 1, wherein the pulse-generating system includes a first two-way valve and a second two-way valve, the first two-way valve being coupled to the gas source and to the vitrector, and the second two-way valve being coupled to the vitrector and to atmosphere.
4. The system of claim 3, wherein, at the first time in the cycle, the first two-way valve opens for a first period of time to raise the pressure at the vitrector to the maximum pressure, the maximum pressure being equal to a first threshold pressure to close the cutting mechanism of the vitrector, and, at the

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second time in the cycle, the second two-way valve opens for a second period of time to reduce the pressure at the vitrector to the minimum pressure, the minimum pressure being equal to a second threshold pressure to allow the cutting mechanism to open.

5. The system of claim 4, wherein the second two-way valve opens after a delay after the first two-way valve closes.

6. The system of claim 1, wherein the gas source is a portable gas canister having a size of approximately 12 g to 33 g.

7. The system of claim 1, further comprising tubing that directs gas to the vitrector, the tubing being maintained at least at the minimum pressure.

8. The system of claim 7, wherein the tubing has a given length, and for the given length, the tubing has a selected inner diameter that minimizes air flow while allowing the vitrector to operate at a range of selectable cut speeds.

9. A method for vitrectomy, comprising:

providing a pulse-generating system with gas from a gas source; and

generating pulses from the pulse-generating system at a vitrector, the vitrector including a cutting mechanism, the pulses causing the pressure at the vitrector to vary according to a cycle, the varying pressure and a spring force at the vitrector causing the cutting mechanism of the vitrector to open and close, the act of generating pulses including:

raising, at a first time in the cycle, the pressure at the vitrector to a maximum pressure by the generation of a pulse by the pulse-generating system to close the cutting mechanism, and

reducing, at a second time in the cycle, the pressure at the vitrector to a minimum pressure that is greater than ambient, the pressure at the vitrector being maintained at least at the minimum pressure and the spring force causing the cutting mechanism to open.

10. The method of claim 9, wherein the pulse-generating system includes a first valve and a second valve, the first valve and the second valve being operable to raise and reduce the pressure at the vitrector according to the cycle.

11. The method of claim 9, wherein the pulse-generating system includes a first two-way valve and a second two-way valve, the first two-way valve being coupled to the gas source and to the vitrector, and the second two-way valve being coupled to the vitrector and to atmosphere.

12. The method of claim 11, wherein the act of generating pulses includes:

at the first time in the cycle, opening the first two-way valve for a first period of time to raise the pressure at the vitrector to the maximum pressure, the maximum pressure being equal to a first threshold pressure to close the cutting mechanism of the vitrector, and

at the second time in the cycle, opening the second two-way valve for a second period of time to reduce the pressure at the vitrector to the minimum pressure, the minimum pressure being equal to a second threshold pressure to allow the cutting mechanism to open.

13. The method of claim 12, wherein the act of generating pulses includes opening the second two-way valve opens after a delay of approximately 8 ms after the first two-way valve closes.

14. The method of claim 9, wherein the gas source is a portable gas canister having a size of approximately 12 g to 33 g.

15. The method of claim 9, wherein the pulse generating system includes tubing that directs gas to the vitrector, the tubing being maintained at least at the minimum pressure.

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16. The method of claim 15, further comprising wherein the tubing has a given length, and for the given length, the tubing has a selected inner diameter that minimizes air flow while allowing the vitrector to operate at a range of selectable cut speeds.

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17. A system for conducting a vitrectomy, comprising:

a gas source;

a vitrector including a cutting mechanism that opens and close according to a pressure at the vitrector; and

a pulse-generating system receiving gas from the gas source and generating at the vitrector, the pulses causing the pressure at the vitrector to vary according to a cycle, the cycle including only a single pulse, the varying pressure at the vitrector causing the cutting mechanism of the vitrector to open and close,

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wherein, at a first time in the cycle, the pulse-generating system generates the single pulse and raises the pressure at the vitrector to a maximum pressure, and

at a second time in the cycle, the pulse-generating system reduces the pressure at the vitrector to a minimum pressure that is greater than ambient, the pressure at the vitrector being maintained at least at the minimum pressure.

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UNITED STATES PATENT AND TRADEMARK OFFICE
CERTIFICATE OF CORRECTION

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APPLICATION NO. : 13/944666
DATED : July 5, 2016
INVENTOR(S) : James C. Easley

Page 1 of 1

It is certified that error appears in the above-identified patent and that said Letters Patent is hereby corrected as shown below:


In the Claims:

At Column 15, Line 41 (Claim 1, Line 9), after “a cycle,” please delete “the varying pressure and a spring force” and insert --the varying pressure and the spring force-- therefor;

At Column 15, Lines 44-47 (Claim 1, Lines 12-15), please delete “the pulse-generating system, generates a pulse and raises the pressure at the vitrector to a maximum pressure, to close the cutting mechanism, and” and insert --the pulse-generating system generates a pulse and raises the pressure at the vitrector to a maximum pressure to close the cutting mechanism, and-- therefor; and,

At Column 17, Line 9 (Claim 17, Line 4), delete “close” and insert --closes-- therefor.

Signed and Sealed this
Fourth Day of October, 2016



Michelle K. Lee
Director of the United States Patent and Trademark Office